Multi-Scale Simulations of the Mechanics of Transport and Growth in Soft Tissue

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Broad Objectives

- mathematical and computational models of the processes of tissue development
 - models that are thermodynamically valid and physiologically appropriate
- parallel experiments on and characterization of *in vitro* engineered tissue
 - quantitative model motivated and validated by experiment
 - model drives the controlled experiments

Development of Biological Tissue

distinct, mathematically independent processes: [Taber - 1995]

- growth addition/loss of mass
 - densification of bone
- remodelling change in microstructure
 - alignment of trabeculae of bones to axis of external loading
- morphogenesis change in macroscopic form
 - development of an embryo from a fertilized egg

Tissue Engineering

engineered tissue *invitro* that is morphologically and functionally similar to neonatal tissue: [Calve et al., 2003]



Tissue Engineering

- capability to engineer constructs which model real tissue
- carefully control environment and apply stimuli to control growth and remodelling
 - mechanical loading in bioreactors
 - chemical environment and nutrient supply

The Issues that Arise

- open system (with respect to mass)
- interacting and interconverting species
- species diffusing with respect to a solid phase
 - fluid, precursors, byproducts
- mixture physics

our treatment involves the introduction of sources, sinks and fluxes of mass

Modelling – Background

- Cowin and Hegedus [1976]: solid tissue; mass source; irreversible sources of momentum and energy from perfusing fluid
- Epstein and Maugin [2000]: mass flux; irreversible fluxes of momentum and entropy
- Kuhl and Steinmann [2002]: configurational forces motivate mass flux
- Baaijens et al. [2004]: detail biosynthesis, enzyme kinetics

Modelling – This Work

- multiple species undergoing transport, interconversion, mechanical and thermodynamic interactions
- other species deform with solid phase and diffuse with respect to it
- fully compatible with mixture theory
- detailed coupling of mechanics and mass balance
- thermodynamic consistency
- preliminary coupled computations

Balance of Mass



- tissue formed by reacting species sources and sinks for species
- transport of precursors, fluid and byproducts fluxes for species

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Balance of Mass – Equations

for a species ι , in local form, in Ω_0

$$\frac{\partial \rho_0^{\iota}}{\partial t} = \Pi^{\iota} - \boldsymbol{\nabla}_X \cdot \boldsymbol{M}^{\iota}, \; \forall \, \iota = \alpha, \dots, \omega$$

the sources/sinks satisfy

$$\sum_{\iota=\alpha}^{\omega} \Pi^{\iota} = 0.$$

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Balance of Mass – Equations

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$$\frac{\partial \rho_0^{\iota}}{\partial t} = \Pi^{\iota} - \boldsymbol{\nabla}_X \cdot \boldsymbol{M}^{\iota}, \; \forall \, \iota = \alpha, \dots, \omega$$

for the solid phase

$$\frac{\partial \rho_0^s}{\partial t} = \Pi^s$$

ignoring short range motion of cells; e.g., during initial stages of wound healing

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Balance of Mass – Equations

for a species ι , in local form, in Ω_0

$$\frac{\partial \rho_0^{\iota}}{\partial t} = \Pi^{\iota} - \boldsymbol{\nabla}_X \cdot \boldsymbol{M}^{\iota}, \; \forall \, \iota = \alpha, \dots, \omega$$

for the fluid phase

$$\frac{\partial \rho_0^f}{\partial t} = -\boldsymbol{\nabla}_X \cdot \boldsymbol{M}^f$$

if sources for interstitial fluids are absent; e.g., no lymph glands

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Balance of Linear Momentum



- linear momentum balance coupled with mass transport sources/sinks and fluxes contribute to the momenta
- material velocity relative to the solid $m{V}^{\iota}=(1/
 ho_{0}^{\iota})m{F}m{M}^{\iota}$

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for a species ι , in local form, in Ω_0

$$\rho_0^{\iota} \frac{\partial}{\partial t} \left(\boldsymbol{V} + \boldsymbol{V}^{\iota} \right) = \rho_0^{\iota} \left(\boldsymbol{g} + \boldsymbol{q}^{\iota} \right) + \boldsymbol{\nabla}_X \cdot \boldsymbol{P}^{\iota} - \left(\boldsymbol{\nabla}_X \left(\boldsymbol{V} + \boldsymbol{V}^{\iota} \right) \right) \boldsymbol{M}^{\iota}, \; \forall \, \iota = \alpha, \dots, \omega$$

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relation between mass sources Π^{ι} 's and interaction forces $oldsymbol{q}^{\iota}$'s,

$$\sum_{\iota=\alpha}^{\omega} \left(\rho_0^{\iota} \boldsymbol{q}^{\iota} + \Pi^{\iota} \boldsymbol{V}^{\iota} \right) = 0$$

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Kinematics of Growth



Kinematics of Growth

$$oldsymbol{F}=ar{oldsymbol{F}}^{\mathrm{e}}{}^{\mathrm{e}}{}^{oldsymbol{F}}{}^{\mathrm{e}}{}^{\iota}oldsymbol{F}^{\mathrm{g}}{}^{\iota}$$

- $F^{g^{\iota}}$ is a kinematic "growth" tensor , $F^{e^{\iota}} = \bar{F}^{e}\tilde{F}^{e^{\iota}}$ is the elastic deformation gradient
- residual stress due to $ilde{m{F}}^{ ext{e}^{\iota}}$

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balance of energy for a species ι , in local form, in Ω_0

$$\rho_0^{\iota} \frac{\partial e^{\iota}}{\partial t} = \boldsymbol{P}^{\iota} : \dot{\boldsymbol{F}} + \boldsymbol{P}^{\iota} : \boldsymbol{\nabla}_X \boldsymbol{V}^{\iota} - \boldsymbol{\nabla}_X \cdot \boldsymbol{Q}^{\iota} + r_0^{\iota} + \rho_0^{\iota} \tilde{e}^{\iota} - \boldsymbol{\nabla}_X e^{\iota} \cdot (\boldsymbol{M}^{\iota})$$

balance of energy for a species ι , in local form, in Ω_0

$$\rho_0^{\iota} \frac{\partial e^{\iota}}{\partial t} = \boldsymbol{P}^{\iota} : \dot{\boldsymbol{F}} + \boldsymbol{P}^{\iota} : \boldsymbol{\nabla}_X \boldsymbol{V}^{\iota} - \boldsymbol{\nabla}_X \cdot \boldsymbol{Q}^{\iota} + r_0^{\iota} + \rho_0^{\iota} \tilde{e}^{\iota} - \boldsymbol{\nabla}_X e^{\iota} \cdot (\boldsymbol{M}^{\iota})$$

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balance of energy for a species ι , in local form, in Ω_0

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where the interaction terms satisfy the relation,

$$\sum_{\iota=\alpha}^{\omega} \left(\rho_0^{\iota} \boldsymbol{q}^{\iota} \cdot (\boldsymbol{V} + \boldsymbol{V}^{\iota}) + \Pi^{\iota} \left(e^{\iota} + \frac{1}{2} \|\boldsymbol{V} + \boldsymbol{V}^{\iota}\|^2 \right) + \rho_0^{\iota} \tilde{e}^{\iota} \right) = 0$$

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Entropy – Second Law

$$\sum_{\iota=\alpha}^{\omega} \rho_0^{\iota} \frac{\partial \eta^{\iota}}{\partial t} \ge \sum_{\iota=\alpha}^{\omega} \left(\frac{r^{\iota}}{\theta} - \boldsymbol{\nabla}_X \eta^{\iota} \cdot \boldsymbol{M}^{\iota} - \frac{\boldsymbol{\nabla}_X \cdot \boldsymbol{Q}^{\iota}}{\theta} + \frac{\boldsymbol{\nabla}_X \theta \cdot \boldsymbol{Q}^{\iota}}{\theta^2} \right)$$

combine first and second laws to get the dissipation inequality

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constitutive hypothesis: $e^{\iota} = \hat{e}^{\iota}(\boldsymbol{F}^{e^{\iota}}, \rho_0^{\iota}, \eta^{\iota})$

constitutive relations consistent with the dissipation inequality:

 $\begin{array}{lll} \boldsymbol{P}^{\iota} = & \rho_{0}^{\iota} \frac{\partial e^{\iota}}{\partial \boldsymbol{F}^{e^{\iota}}}, \forall \, \iota & \circ \text{ hyperelastic material} \\ \\ \theta = & \frac{\partial e^{\iota}}{\partial \eta^{\iota}}, \forall \, \iota & \circ \text{ thermal physics} \\ \\ \boldsymbol{Q}^{\iota} = & -\boldsymbol{K}^{\iota} \boldsymbol{\nabla}_{X} \theta, \forall \, \iota & \circ \text{ fourier law} \\ \\ \boldsymbol{u} \cdot \boldsymbol{K}^{\iota} \boldsymbol{u} \geq & 0 \, \forall \boldsymbol{u} \in \mathbb{R}^{3} & (\text{semi-positive definite conductivity}) \end{array}$

constitutive relation for flux of each transported species:

$$egin{aligned} m{M}^{\iota} &= m{D}^{\iota} \left(-
ho_0^{\iota} m{F}^{\mathrm{T}} rac{\partial m{V}}{\partial t} +
ho_0^{\iota} m{F}^{\mathrm{T}} m{g} + m{F}^{\mathrm{T}} m{
abla}_X \cdot m{P}^{\iota} - m{
abla}_X (e^{\iota} - heta \eta^{\iota})
ight) \ & m{u} \cdot m{D}^{\iota} m{u} \geq 0 \, orall m{u} \in \mathbb{R}^3 \end{aligned}$$

 $\circ \, D^{\iota}$ is the mobility

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constitutive relation for flux of each transported species:

$$\boldsymbol{M}^{\iota} = \boldsymbol{D}^{\iota} \left(-\rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \frac{\partial \boldsymbol{V}}{\partial t} + \rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \boldsymbol{g} + \boldsymbol{F}^{\mathrm{T}} \boldsymbol{\nabla}_{X} \cdot \boldsymbol{P}^{\iota} - \boldsymbol{\nabla}_{X} (e^{\iota} - \theta \eta^{\iota}) \right)$$

• driving force due to inertia

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constitutive relation for flux of each transported species:

$$\boldsymbol{M}^{\iota} = \boldsymbol{D}^{\iota} \left(-\rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \frac{\partial \boldsymbol{V}}{\partial t} + \rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \boldsymbol{g} + \boldsymbol{F}^{\mathrm{T}} \boldsymbol{\nabla}_{X} \cdot \boldsymbol{P}^{\iota} - \boldsymbol{\nabla}_{X} (e^{\iota} - \theta \eta^{\iota}) \right)$$

• driving force due to gravity

constitutive relation for flux of each transported species:

$$\boldsymbol{M}^{\iota} = \boldsymbol{D}^{\iota} \left(-\rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \frac{\partial \boldsymbol{V}}{\partial t} + \rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \boldsymbol{g} + \boldsymbol{F}^{\mathrm{T}} \boldsymbol{\nabla}_{X} \cdot \boldsymbol{P}^{\iota} - \boldsymbol{\nabla}_{X} (e^{\iota} - \theta \eta^{\iota}) \right)$$

• driving force due to stress gradient – Darcy's law

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constitutive relation for flux of each transported species:

$$\boldsymbol{M}^{\iota} = \boldsymbol{D}^{\iota} \left(-\rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \frac{\partial \boldsymbol{V}}{\partial t} + \rho_{0}^{\iota} \boldsymbol{F}^{\mathrm{T}} \boldsymbol{g} + \boldsymbol{F}^{\mathrm{T}} \boldsymbol{\nabla}_{X} \cdot \boldsymbol{P}^{\iota} - \boldsymbol{\nabla}_{X} (e^{\iota} - \theta \eta^{\iota}) \right)$$

• driving force due to a chemical potential gradient

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constitutive relation for flux of each transported precursor/byproduct:

$$\tilde{\boldsymbol{M}}^{\iota} = \boldsymbol{D}^{\iota} \left(-\rho_0^{\iota} \boldsymbol{F}^{\mathrm{T}} \frac{\partial (\boldsymbol{V} + \boldsymbol{V}^{\iota})}{\partial t} + \rho_0^{\iota} \boldsymbol{F}^{\mathrm{T}} \boldsymbol{g} - \boldsymbol{\nabla}_X (e^{\iota} - \theta \eta^{\iota}) \right)$$

Reduced Dissipation Inequality

with the constitutive relations ensuring the non-positiveness of certain terms, the entropy inequality is reduced to

$$\mathcal{D} = \sum_{\iota=\alpha}^{\omega} \left(\rho_0^{\iota} \frac{\partial e^{\iota}}{\partial \rho_0^{\iota}} \frac{\partial \rho_0^{\iota}}{\partial t} - \boldsymbol{P}^{\iota} : \boldsymbol{\nabla}_X \boldsymbol{V}^{\iota} + \rho_0^{\iota} \boldsymbol{V}^{\iota} \cdot \left(\frac{\partial \boldsymbol{V}^{\iota}}{\partial t} + (\boldsymbol{\nabla}_X \boldsymbol{V}^{\iota}) \boldsymbol{F}^{-1} \boldsymbol{V}^{\iota} \right) \right) \\ + \sum_{\iota=\alpha}^{\omega} \Pi^{\iota} \left(e^{\iota} + \frac{1}{2} \| \boldsymbol{V} + \boldsymbol{V}^{\iota} \|^2 \right) \\ + \sum_{\iota=\alpha}^{\omega} \left(\rho_0^{\iota} \frac{\partial}{\partial t} \left(\boldsymbol{V} + \boldsymbol{V}^{\iota} \right) - \rho_0^{\iota} \boldsymbol{g} - \boldsymbol{\nabla}_X \cdot \boldsymbol{P}^{\iota} + \boldsymbol{\nabla}_X \left(\boldsymbol{V} + \boldsymbol{V}^{\iota} \right) \left(\rho_0^{\iota} \boldsymbol{F}^{-1} \boldsymbol{V}^{\iota} \right) \right) \cdot \boldsymbol{V} \le 0$$

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Computational Formulation

- Implementation in FEAP
- Coupled implementation; staggered scheme (Armero [1999], Garikipati et al. [2001])
- Nonlinear projection methods to treat incompressibility (Simo et al. [1985])
- Energy-momentum conserving algorithm for dynamics (Simo & Tarnow [1992a,b])

Computational Formulation

- Backward Euler for time-dependent mass balance
- Mixed method for stress/strain gradient-driven fluxes (Garikipati et al. [2001])
- Large advective terms require stabilization

Coupled Computations – Examples

- biphasic model
 - worm-like chain model for collagen
 - $\circ\,$ ideal, nearly incompressible interstitial fluid with bulk compressibility of water, $\pmb{\kappa}^{\rm f}=2.25~{\rm GPa}$
- "artificial" sources:

$$\Pi^{\rm f} = -k^{\rm f} (\rho_0^{\rm f} - \rho_{0_{\rm ini}}^{\rm f}), \quad \Pi^{\rm s} = -\Pi^{\rm f}$$

• entropy of mixing:

$$\eta_{\rm mix}^{\iota} = -\frac{k}{\mathcal{M}^{\iota}}\log\frac{\rho_0^{\iota}}{\rho_0}$$

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Coupled Computations – Examples – Swelling



- fluid concentration evolution
- o fluid sink evolution
- solid concentration evolution

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Coupled Computations – Examples – Pinching

Time = 0.00E+00





Time = 1.00E+01

- o fluid concentration evolution
- o fluid sink evolution
- solid concentration evolution

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Summary and Further Work

- physiologically consistent continuum formulation describing growth in an open system
- relevant driving forces arise from thermodynamics coupling with mechanics
- consistent with mixture theory
- formulated a theoretical framework for the remodelling problem
- engineering and characterization of growing, functional biological tissue

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Worm-like Chain Model for Solid Collagen

$$\begin{array}{c|c} & & & \\$$

$$r = \frac{1}{2}\sqrt{a^2\lambda_1^{e^2} + b^2\lambda_2^{e^2} + c^2\lambda_3^{e^2}}, \quad \lambda_I^e = \sqrt{\boldsymbol{N}_I \cdot \boldsymbol{C}^e \boldsymbol{N}_I}$$

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